



Australian Government

Patent Office  
Canberra

I, MICHELLE HENKEL, TEAM LEADER EXAMINATION SUPPORT AND SALES hereby certify that annexed is a true copy of the Provisional specification in connection with Application No. 2002951739 for a patent by COCHLEAR LIMITED as filed on 30 September 2002.

WITNESS my hand this  
Fourteenth day of February 2006

A handwritten signature in cursive script that reads "Michelle Henkel".

MICHELLE HENKEL  
TEAM LEADER EXAMINATION  
SUPPORT AND SALES



CERTIFIED COPY OF  
PRIORITY DOCUMENT

# AUSTRALIA

## Patents Act 1990

Cochlear Limited

### PROVISIONAL SPECIFICATION

*Invention Title:*

*Feedthrough with multiple conductive pathways extending  
therethrough*

The invention is described in the following statement:

### Field of the Invention

The present invention relates to an electrical connector system for electrical products. More specifically, the present invention relates to an electrical connector having one or more hermetically sealed but electrically conducting feedthroughs extending therethrough. The connector can be used in devices such as biosensors and implantable devices. Examples of implantable devices include the implantable component of a cochlear implant hearing prosthesis.

10

### Background of the Invention

The term 'feedthrough' as used herein refers to the provision of an electrically conducting path extending from the interior of a hermetically sealed container or housing to an external location outside the container or housing. Typically, a conductive path is provided through the feedthrough by an electrically conductive pin, which is electrically insulated from the container or housing by an electrically insulating body surrounding the pin.

A feedthrough device therefore allows one or more electrical connections to be made with electronic circuitry or components within the hermetically sealed container or housing, whilst protecting the circuitry or components from any damage or malfunction that may result from exposure to the surrounding environment.

25

There are many applications that require feedthrough devices to provide an electrically conducting path whilst also sealing the electrical container or housing from its ambient environment. Historically, the first such devices were widely used in vacuum technology allowing for the transfer of signals between chambers of differing pressures. In such applications, the vacuum tubes had to be sealed because they could only operate under low-pressure conditions.

Over time, and with the advent of electrical devices capable of being implanted in body tissue to provide therapy to a patient, such as cardiac pacemakers, defibrillators and cochlear implants, the need to provide feedthrough devices with improved hermeticity has become increasingly

35

important. As the environment of living tissue and body fluids is quite corrosive and the implants may contain materials which may be detrimental to the patient, a hermetic feedthrough device is used to provide a barrier between the electronic components of the device and the external corrosive environment of the human body. With implantable medical devices in particular, it is critically important that the hermetic seal of the device be physically rugged and long lasting. For this reason, stringent requirements are imposed on the hermeticity of an implanted device, typically requiring a seal that provides a leakage rate of less than  $10^{-8}$  cc/sec.

10

In this regard, in medical implant applications such as those used in pacemaker devices and cochlear implants, the feedthroughs typically consist of a ceramic or glass bead that is bonded chemically at its perimeter through brazing or the use of oxides, and/or mechanically bonded through compression, to the walls of the sealed package. A suitable wire or other conductor passes through the centre of the bead, and this wire or conductor must also be sealed to the bead through chemical bonds and or mechanical compression. In this regard, the feedthrough is typically cylindrical and the wire(s) or conductor(s) mounted within the bead are centred or mounted in a uniform pattern, centrally within the bead.

20

Other materials and processes are known for making feedthroughs, for example, from aluminium oxide ceramic and binders. These types of feedthroughs are widely used for cardiac and cochlear implants. One of the processes for making such a feedthrough consists of pre-drilling holes in a sintered ceramic plate and then forcing electrical conductive pins through the holes. However, this method does not necessarily guarantee a hermetic seal, resulting in unsatisfactory leakage rates. A second method involves inserting the conductive pins into an unsintered (or 'green') ceramic plate and then curing the assembly by firing to achieve a hermetic seal. A major disadvantage of this last method is that, historically the manufacturing process has been performed by hand. Such a method of manufacture can lead to inaccuracies and be time consuming, expensive and labour intensive. Moreover, the feedthrough devices resulting from such a process do not necessarily have precisely positioned electrical conductors, with the position of the conductors being greatly dependent upon the process itself. Further, as the conductors

30  
35

are typically wires being of a general cylindrical shape and configuration, the size and shape of the conductor extending from the insulative material of the feedthrough is generally the same as the conductor embedded in the insulative material of the feedthrough. This aspect has made it difficult to design  
5 feedthrough devices wherein the shape of the conductor element differs over the length of the conductor such that the external ends of the conductors are maximised to suit the specific purpose of the feedthrough device.

As implantable devices continue to develop and become thinner and  
10 smaller and more electronically sophisticated, the requirements of the feedthrough have also increased. In cochlear implants in particular, where there are now typically 22-24 electrode leads, there is a need for 22-24 conductive pins passing through the feedthrough device. As the desire for more electrodes and smaller feedthroughs increases, the demands placed  
15 upon the design of the traditional feedthrough also increases. The problems in fabricating such a feedthrough device on such a large scale are therefore quite significant, especially when one considers the relatively high degree of labour intensity and specialisation of the current fabricating methods.

20 While the above described prior art feedthrough devices and fabrication methods have proven successful, it is a relatively slow and labour intensive process to manufacture such devices. The method of manufacture of the feedthrough also presents limitations in the number of conductors that can pass through the feedthrough and the position and configuration of such conductors  
25 within the feedthrough device, particularly in applications where this number needs to be maximised.

The present invention is directed to an alternative design for a connector and electrically conducting feedthrough arrangement having features that  
30 hitherto have not been offered by the existing feedthrough designs.

Any discussion of documents, acts, materials, devices, articles or the like which has been included in the present specification is solely for the purpose of providing a context for the present invention. It is not to be taken as an  
35 admission that any or all of these matters form part of the prior art base or were

common general knowledge in the field relevant to the present invention as it existed before the priority date of each claim of this application.

### Summary of the Invention

5

Throughout this specification the word "comprise", or variations such as "comprises" or "comprising", will be understood to imply the inclusion of a stated element, integer or step, or group of elements, integers or steps, but not the exclusion of any other element, integer or step, or group of elements, integers or steps.

According to a first aspect, the present invention is an electrically conducting feedthrough comprising:

a relatively electrically insulative member having a first face and at least a second face; and

two or more groups of electrically conductive members, each conductive member having a first end and a second end and extending through at least a portion of the insulative member from said first end at or adjacent the first face to said second end at or adjacent the second face of the insulative member;

each group comprising an array of conductive members.

The electrically insulative member is preferably formed from a ceramic material or hermetic glass material, suitable for use in a feedthrough application.

25

In one embodiment, the electrically conductive members can be formed from a film or shim of an electrically conductive metal or metal alloy. In a preferred embodiment, the film or shim is formed from a biocompatible metal or metal alloy. In one such embodiment, the electrically conductive structure can be formed from a film or shim of platinum.

In a further embodiment, each conductive member in a group can be identical in configuration to the other conductive members in a group. In another embodiment, at least one conductive member in a group can be different in configuration to one or all of the other conductive members in that group. In another embodiment, the conductive members of one group can be

different in configuration to one or more of the conductive members of another group of the feedthrough. Still further, the conductive members of one group can be identical in configuration to one or more of the conductive members of another group of the feedthrough.

5

In one embodiment, each feedthrough comprises two, three or more groups of conductive members. Each group can comprise a series of conductive members in side-by-side relationship. In this regard, the conductive members can be in a parallel arrangement.

10

In one embodiment, each conductive member has an elongate length of at least 7mm, more preferably 7.8mm. The conductive members can further have a width of between 1.5 and 2.5mm. In a still further embodiment, the film or shim from which the conductive members are formed can have a thickness  
15 of between about 40 and 70 microns, more preferably about 50 microns.

In one embodiment, the configuration of the first ends of the conductive members at or adjacent the first face of the insulative member is different to the configuration of the second ends of the conductive members at or adjacent the  
20 second face of the insulative member.

In this embodiment, the respective configurations of the first ends and the second ends of the conductive members can be such that the number of first ends of the conductive members per a defined unit area at or adjacent the  
25 first face of the insulative member is different to the number of second ends of the conductive members per said defined unit area at or adjacent the second face of the insulative member.

In one embodiment, the number of first ends per defined unit area can be  
30 greater than the number of second ends per said defined unit area. In another embodiment, the number of first ends per defined unit area can be less than the number of second ends per said defined unit area.

In this embodiment, the defined unit area can be  $1\text{mm}^2$ ,  $1\text{cm}^2$ , or some  
35 other area.

Still further, the respective configurations of the first ends and the second ends of the conductive members can be such that the spacing between the first ends of the conductive members at or adjacent the first face of the insulative member is different to the spacing between the second ends of the conductive members at or adjacent the second face of the insulative member.

In this embodiment, the spacing between the first ends of the conductive members can be greater than the spacing between the second ends of the conductive members. In another embodiment, the spacing between the first ends of the conductive members can be less than the spacing between the second ends of the conductive members.

In one embodiment, the spacing between respective groups of first ends at or adjacent the first end can be different to the spacing between respective groups of second ends at or adjacent the second face. In this embodiment, the spacing between the first ends within a group can be the same or different to the spacing of the second ends of this group of conductive members.

In yet another embodiment, the respective dimensions and shape of the first ends and second ends of the conductive members can be such that their shape and dimensions can differ between the first ends at or adjacent the first face of the insulative member and the second ends at or adjacent the second face of the insulative member. Equally, the shape and dimensions of the first and second ends of the conductive members can also differ from the shape and dimensions of the conductive member embedded within the insulative member.

In this embodiment, the shape and dimensions of the first ends of the conductive members can be such as to allow the ends to communicate directly with an integrated chip design whilst the shape and dimensions of the second ends of the conductive members can be such as to allow the ends to communicate with wires/leads connected to a stimulating electrode or the like. In this regard, the size and shape of the first and second ends of the conductive members can be determined prior to the manufacturing of the feedthrough device.

One or more of said conductive members can be non-linear. In another embodiment, one or more of the conductive members can have a length between said first face and second face that is greater than the shortest distance between said first face and said second face. In another embodiment,  
5 the interface between one or more of the conductive members and the insulative member can be non-linear.

In a further embodiment, the length of the conductive members of each group are different to the length of the members in an adjacent group. Each of  
10 the members in a group can have the same length. In another embodiment, the members within a group can be of different lengths. The conductive members of a group are also offset from its adjacent groups. In a feedthrough, the groups can be in a parallel relationship or a non-parallel relationship. Each of the conductive members can be linear and parallel to other members within  
15 its group or they can be non-parallel and have different configurations

The present invention offers the capability of the feedthrough having a plurality of layers of conductive members. Such layers of conductive members can be off-set from adjacent layers.

20

In one embodiment, the first face and second face of the insulative member can face outwardly in opposite directions. In one embodiment, the first and second faces can be substantially parallel or parallel. The first face is preferably the outer face of the feedthrough and the second face is preferably  
25 the inner face of the feedthrough.

In a further embodiment, said one or more conductive members can undergo a first change of direction between the first face and the second face of the insulative member. In another embodiment, said one or more conductive  
30 members can undergo two or more changes of direction between the first face and the second face of the insulative member.

In yet another embodiment, said one or more conductive members undergo a change of direction in a nominal plane extending at an angle, such  
35 as a right angle, to one or both faces of the insulative member. In another embodiment, said one or more conductive members can undergo a change of

direction into a direction out of a nominal plane extending at an angle, such as a right angle, to one or both faces of the insulative member. The conductive member can undergo more than one change of direction out of said nominal plane.

5

Each change of direction can be at a right angle to the preceding direction of the conductive member. In another embodiment, the change of direction can be at a different angle than a right angle to that of the preceding direction.

10

In another embodiment, the change of direction can be abrupt. In another embodiment, the change of direction can be smoothly curved. In another embodiment, a particular conductive member can undergo a combination of abrupt and/or smoothly curved changes of direction.

15

In one embodiment, a feedthrough according to the present invention can be formed using a method comprising the steps of:

(i) forming two or more electrically conductive structures comprising a sacrificial component and non-sacrificial component;

20 (ii) placing the two or more groups in a desired configuration adjacent each other;

(ii) coating a relatively electrically insulative member on to at least a portion of the non-sacrificial component of the two or more structures; and

25 (iii) removing at least a portion of the sacrificial component of each structure.

In this embodiment, the electrically conductive structures can be formed from a film or shim of platinum that is formed into a shape comprising the sacrificial component and the non-sacrificial component of the electrically  
30 conductive structure. In this embodiment, it will be appreciated that that portion of the film or shim comprising the non-sacrificial component may comprise more than one portion of the film or shim. Similarly, that portion of the film or shim comprising the sacrificial component may comprise more than one portion of the film or shim.

35

In one embodiment, each electrically conductive component may comprise a film or shim having a shape comprising a plurality of separated members extending between respective transverse support members. In a further embodiment, the film or shim can have at least ten separated members  
5 extending between the respective support members. In a further embodiment, the support members can be in a side-by-side relationship with respect to each other.

The separation of the members is preferably such that the insulative  
10 member material can be coated between the members and so prevent electrical conduction between the respective members at completion of the method as defined herein.

In a preferred embodiment, the shape of each electrically conductive  
15 component comprising what will become the conductive members can be formed in step (i) by punching the shape, using a suitable shaped and dimensioned punching tool, from a film of platinum. Each conductive component of a particular feedthrough may be identical or different with respect to each other.

20

In another embodiment, the shape of each electrically conductive component can be formed in step (i) by using electrical discharge machining (EDM), which is also known as spark erosion, to remove unwanted portions of the sheet. In a preferred embodiment, the EDM equipment used in the process  
25 has a cutting tool comprising an electrode. The cutting tool does not physically cut the sheet but instead relies on the equipment generating a series of electrical discharges between the electrode and the sheet in a dielectric fluid. The electrical discharges serve to vaporise the sheet in the region adjacent the cutting tool.

30

In a preferred embodiment, the cutting tool has a size and shape that matches the size and shape of the portion of the sheet to be removed from the sheet during the machining steps. In this embodiment, it is preferred that the tool is brought adjacent the sheet at a number of different locations so as to  
35 remove differing portions of the sheet. This multiple use of the tool preferably

serves to gradually build up the pattern of the electrically conductive component comprising the conductive members.

5 In a preferred embodiment, the cutting tool can be used to form a series of discrete conductive members from a sheet of platinum or other suitable metal. The conductive members are preferably disposed in a side-by-side arrangement.

10 In another embodiment, the cutting tool can be used to form a series of discrete conductive members from a plurality of sheets of platinum or other suitable material stacked one atop the other. In this manner, a large number of electrically conductive components can be prepared with a single cutting motion of the cutting tool. In such an embodiment, a method known as "wire cutting" can be employed. This method operates in a similar manner to  
15 EDM/spark erosion methods wherein a wire is passed through a stack of sheets or foils of conductive material with this wire becoming the electrode causing the erosion of material adjacent the electrode. By using this method a plurality of foils can be patterned simultaneously, resulting in a process that is capable of mass producing patterned conductive foils to be used to create the  
20 feedthrough device of the present invention.

In this embodiment, at least a portion of each of the members extending between the support members are coated with the insulative member material. The insulative material can be alumina but other suitable ceramic types can be  
25 envisaged.

In one embodiment, the insulative member material can be coated on the non-sacrificial component and not coated or moulded on to at least a portion of the sacrificial component of the conductive structure. Still further, step (iii) of  
30 the method can comprise removing at least that portion of the sacrificial component on to which the insulative member has not been coated.

The step of coating the electrically conductive structure preferably comprises a first step of mounting or clamping the two or more conductive  
35 structures in an appropriate and desired adjacent configuration in a mould and

then moulding a coating of the insulative material on and/or around the conductive structures.

Where the conductive structures comprise a plurality of conductive members formed from a film or shim of platinum, the insulative material is preferably coated or moulded around at least a portion of the members of each conductive structure. In this embodiment, said portion of the members comprises a portion of the non-sacrificial component of the electrically conductive structure. While this embodiment envisages the film or shim being shaped as desired prior to clamping or mounting in the mould, it will be appreciated that a film could be firstly mounted or clamped in the mould and then shaped or punched as required prior to the moulding or coating step.

In a preferred embodiment, the mould can comprise an injection mould. In one embodiment, step (ii) can comprise a step of using powder injection moulding (PIM) to mould the insulative material around the desired portion of the conductive structure.

In this moulding process, insulative material, such as fine ceramic powder, is mixed with a carrier chemical, typically called binder, and homogenised to create a feedstock for the injection mould. The presence of the binder serves to make the feedstock sufficiently fluid to be used in an injection moulding process. Once moulded, the insulative material can be allowed to at least partially set. The resulting moulded part is hereinafter called the green body.

Once the green body is formed, the sacrificial component of each electrically conductive structure can be removed. During this step, it is possible that a portion of the green body may also need to be removed. In one embodiment, the sacrificial component can be removed by being cut, abraded or ground away. In this regard, physical cutting with a knife, or laser cutting techniques, are envisaged.

Where each electrically conductive structure comprises the plurality of members extending between the transverse members, the sacrificial

component preferably includes at least the transverse members so leaving a plurality of electrically insulated members extending through the green body.

In a still further embodiment, the method can comprise an additional step  
5 of debinding the green body. In this step, any binder in the green body is preferably extracted from the insulative material. In one embodiment, this step can comprise a chemical debinding in which the green body is soaked in a suitable solvent. In another embodiment, this step can comprise exposing the green body to a relatively elevated temperature. This temperature is preferably  
10 sufficient to boil off the binder from the green body while not causing the green body to undergo sintering. In one embodiment, the temperature is between about 150°C and 200°C.

During the debinding step, the insulative material preferably shrinks in  
15 dimension. This debinded insulative member is hereinafter called a brown body.

When ready, the brown body can undergo a sintering step. The sintering step preferably comprises exposing the brown body to a suitable elevated  
20 temperature. In one embodiment, the sintering step can comprise exposing the brown body to a sintering temperature of about 1700°C. During the sintering step, the insulative member undergoes further shrinkage and becomes relatively more robust. The shrinkage of the insulative member also serves to form an hermetic seal at the interface between the embedded conductive  
25 members and the surrounding sintered insulative member.

Once complete, the insulative member with the conductive members extending therethrough can be brazed into an orifice in the wall of a unit adapted to receive the feedthrough. Electrical connection can then be made to  
30 each end of the respective platinum members as required to form respective electrical conductive paths through the insulative body of the feedthrough.

In one embodiment, the feedthrough can be brazed into the wall of an electrical device, such as an implantable stimulator unit of a medical implant  
35 device. In a preferred embodiment, the feedthrough can be adapted to be used with a cochlear implant hearing prosthesis to provide electrical conduction

between the circuitry within the implantable stimulator unit and the intracochlear or extracochlear electrodes and/or the implantable receiver coil.

Each feedthrough preferably has sufficient conductive members  
5 embedded therein to ensure there are sufficient connectors to suit the desired application. In a cochlear implant application, the feedthrough would have to have sufficient conductive members embedded therein to ensure that there are sufficient connectors for each of the electrode channels of the intracochlear electrode array, one or more extracochlear electrodes, and the inputs from the  
10 receiver coil.

In one embodiment, the present invention is a feedthrough for an implantable component comprising an insulative member having a plurality of electrically conductive members extending therethrough. The conductive  
15 members are hermetically encased within the insulative member in a way that allows electrical connection through the feedthrough while preventing transfer of bodily fluids from outside the component into the interior of the component.

#### Brief Description of the Drawings

20

By way of example only, a preferred embodiment of the invention is now described with reference to the accompanying drawings, in which:

Fig. 1 is a plan view of one embodiment of one electrically conductive  
25 structure for use in the manufacture of a feedthrough according to the present invention;

Fig. 2 is a plan view of one embodiment of one electrically conductive structure for use in the manufacture of a feedthrough according to the present  
30 invention;

Fig. 3 is a plan view of one embodiment of one electrically conductive structure for use in the manufacture of a feedthrough according to the present  
35 invention;

Fig. 4 is a plan view of a feedthrough having a plurality of electrically conductive structures of Fig. 1 embedded within a ceramic member;

Fig. 5 is a sectional view of the feedthrough of Fig. 2 depicting the three  
5 groups of conductive members;

Fig. 6 is a sectional view of another embodiment of a feedthrough according to the present invention;

10 Fig. 7 is a sectional view of a still further embodiment of a feedthrough according to the present invention; and

Fig. 8 is a further part-sectional, part front view of the feedthrough of Fig.  
7.

15

#### Preferred Mode of Carrying out the Invention

Figs. 1, 2 and 3 depict different types of electrically conductive structure that can be used in the manufacture of a feedthrough according to the present  
20 invention. Other conductive structures can be envisaged.

The depicted electrically conductive structure in these figures are formed from a film or shim 21 of biocompatible platinum. Other suitable electrically  
25 conductive metals or metal alloys can be envisaged.

25

In each figure, the film or shim 21 of platinum is formed into a shape comprising a sacrificial component and a non-sacrificial component. In this embodiment, the electrically conductive structure comprises a plurality of separated members 22 extending between respective parallel transverse  
30 support members 23,24.

In Fig. 1, the conductive members 22 are linear and disposed in a parallel arrangement.

In Fig. 2, the conductive members 22 are non-linear. In the depicted embodiment, the non-linear members 22 have two relatively abrupt right angle changes of direction at corners 25 and 26.

5 In Fig. 3, the spacing between the conductive members 22 at their connection to transverse member 23 is larger than the spacing between the conductive members where they connect to transverse member 24.

10 While Fig. 3 depicts the members 22 as being straight, it will be appreciated that non-linear members could extend between the respective transverse members 23,24 in this embodiment.

The separation of the members 22 in each embodiment is such that the insulative member, such as a ceramic member, when moulded around the  
15 members 22 can also move between the members 22 and so prevent electrical conduction between the respective members 22.

In the depicted embodiments, the shape of the electrically conductive structure 21 is formed by punching the shape, using a suitable shaped and  
20 dimensioned punching tool, from a film of platinum. It is envisaged that the shape could also be created by a variety of material removal methods, such as electrical discharge machining (EDM), micro-knifing and/or laser cutting.

As is shown in Fig. 1, the ends 50 of the members 22 can have a shape  
25 and dimension different to the portion of the member 22 embedded in the insulative member. Equally, each of the ends 50 of the members 22 may have a shape and dimension different to each other, with said shape and dimension being determined prior to injection moulding of the insulative member and specific to the desired application of the feedthrough device.

30

In the present invention, the step of moulding the insulative member (in the depicted embodiment a ceramic 35) (see Fig. 4) around the electrically conductive structure comprises a step of mounting or clamping two or more conductive structures in an adjacent configuration in a mould and then  
35 moulding the ceramic on and/or around the respective conductive structures.

In Fig. 4, the feedthrough is depicted in plan view and as such only the first group of conductive members 2 is visible. As depicted in Fig. 5, the feedthrough actually comprises three separate groups of conductive structures 22 disposed in a parallel arrangement. While each group of conductive structures depicted in Fig. 5 is made of a conductive structure depicted in Fig. 3, it will be appreciated that the feedthrough could be formed of three conductive structures depicted in Fig. 1 or three conductive structures depicted in Fig. 2. Alternatively, the feedthrough could be formed of one each of the conductive structures depicted in Figs 1, 2 and 3, respectively. Still further, the feedthrough might be formed of two of one structure of either Figs. 1-3 and one of the others depicted in these figures.

As depicted in Fig. 6, the respective groups of conductive structures 22 need not be mounted in a parallel configuration. Again, the respective groups of conductive members 22 can be formed from various combinations of conductive structures as depicted in Figs. 1-3 or other structures within the scope of the invention.

Figs. 7 and 8 depict a further embodiment where the length of the conductive members of each group are different to the length of the members in an adjacent group. The conductive members of a group are also offset from its adjacent groups. While the groups are in a parallel relationship, it will be appreciated that the groups could be in a non-parallel relationship as depicted in Fig. 6. Each of the conductive members are also depicted as linear and parallel to other members within its group. Again, it can be envisaged that instead, the conductive members may have different configurations, such as is depicted in Figs. 2 or 3.

In a preferred embodiment, the mould can comprise an injection mould. In one embodiment, powder injection moulding (PIM) can be used to mould the insulative member material (such as ceramic) around the desired portions of the conductive structures. In this moulding process, fine ceramic powder is mixed with a binder and homogenised to create a feedstock for the injection mould. The presence of the binder serves to make the feedstock sufficiently fluid to be used in an injection moulding process. Once moulded, the ceramic can be allowed to at least partially set and form a green body.

Once the green body is formed, the sacrificial components of the electrically conductive structures can be removed. In the depicted embodiment, the sacrificial component can be removed by laser cutting. Other  
5 suitable material removal techniques, such as cutting or abrading techniques are also envisaged.

In the embodiments depicted in the drawings, the sacrificial component comprises the transverse members 23,24. Once these are removed, a plurality  
10 of respectively electrically insulated members 22 remain extending through the green body 35 as depicted in Fig. 4-8.

The method of forming the feedthrough further comprises a step of debinding the green body. In this step, the binder in the green body is  
15 extracted from the insulative member material. In one embodiment, this step can comprise a chemical debinding in which the green body is soaked in a suitable solvent. In another embodiment, this step can comprise exposing to a relatively elevated temperature. This temperature is preferably sufficient to boil off the binder from the green body while not causing the green body to undergo  
20 sintering. In one embodiment, the temperature is between about 150°C and 200°C.

During the debinding step, the insulative member preferably shrinks in dimension to form a brown body.  
25

When ready, the brown body can undergo a sintering step. The sintering step preferably comprises exposing the brown body to a suitable elevated temperature. In one embodiment, the sintering step can comprise exposing the brown body to a sintering temperature of about 1700°C. During the sintering  
30 step, the insulative member undergoes further shrinkage and becomes relatively more robust. The shrinkage of the insulative member also serves to form an hermetic seal at the interface between the embedded conductive members and the surrounding sintered insulative member.

35 Once complete, the insulative member with the conductive members extending therethrough can be brazed into an orifice in the wall of a unit

adapted to receive the feedthrough. Electrical connection can then be made to each end of the respective conductive members as required to form respective electrical conductive paths through the insulative body of the feedthrough.

5        Such a feedthrough can be adapted to be brazed into the wall of an implantable stimulator unit of a cochlear implant hearing prosthesis. In this embodiment, the feedthrough can be adapted to provide electrical conduction between the circuitry within the implantable stimulator unit and the intracochlear or extracochlear electrodes, and/or the implantable receiver coil.

10

Each feedthrough preferably has sufficient conductive members embedded therein to ensure there are sufficient connectors for each of the electrode channels of the intracochlear electrode array, one or more extracochlear electrodes, and the inputs from the receiver coil.

15

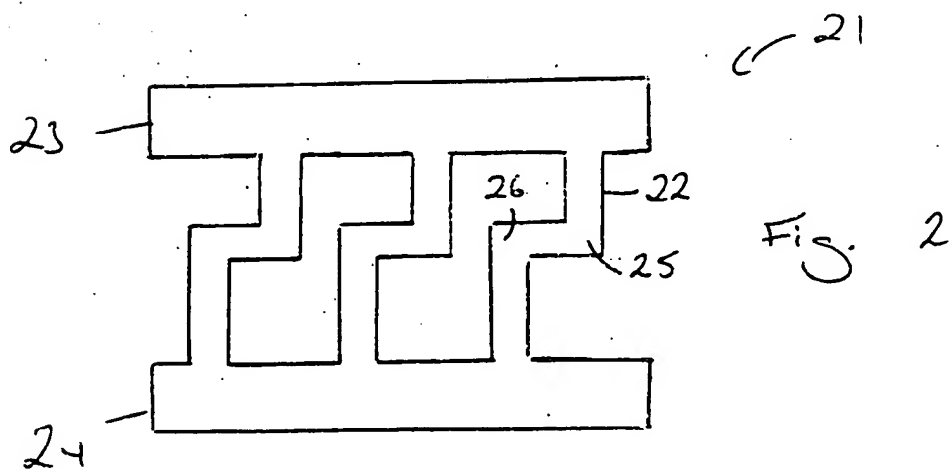
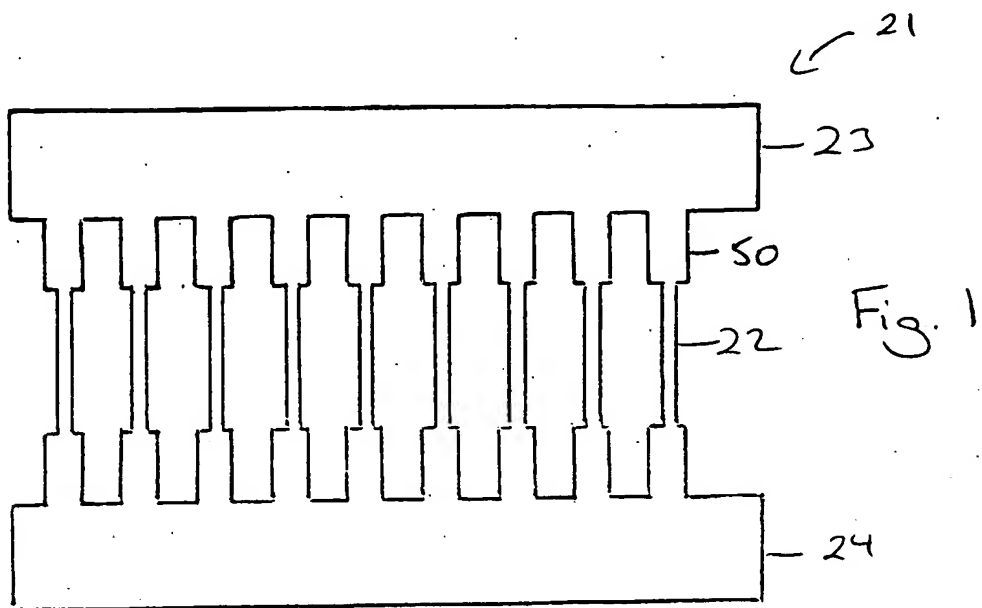
In one embodiment, the present invention is a feedthrough for an implantable component comprising an insulative member having a plurality of electrically conductive members extending therethrough. The method of forming this feedthrough ensures the conductive members have a sufficient  
20 length and are encased within the insulative member in a way that allows electrical connection through the feedthrough while preventing transfer of bodily fluids from outside the component into the interior of the component.

It will be appreciated by persons skilled in the art that numerous  
25 variations and/or modifications may be made to the invention as shown in the specific embodiments without departing from the spirit or scope of the invention as broadly described. The present embodiments are, therefore, to be considered in all respects as illustrative and not restrictive.

Dated this thirtieth day of August 2002

Cochlear Limited  
Patent Attorneys for the Applicant:

F B RICE & CO



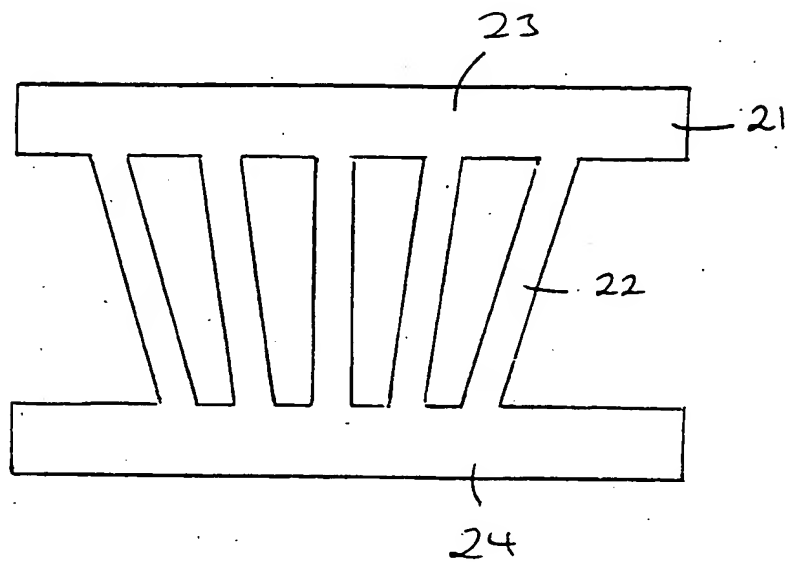


Fig. 3

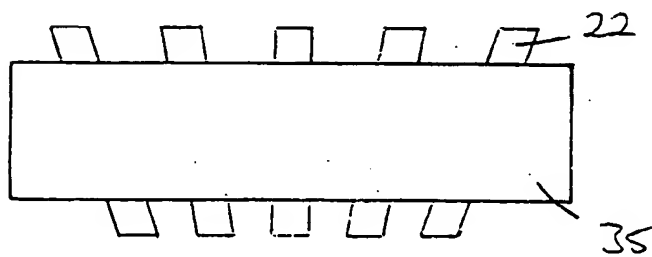


Fig. 4

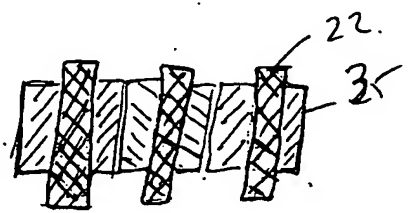


FIG. 5

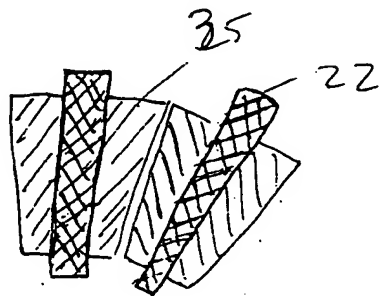


FIG. 6

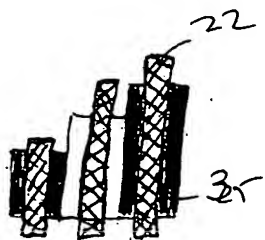


FIG. 7

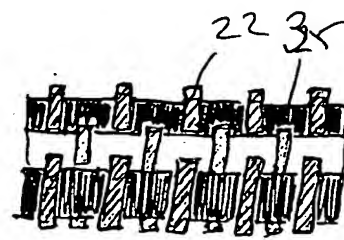


FIG. 8